# Detection and Classification of Levels of Consciousness Using Frontal and Parietal EEG-fNIRS During Deep Sedation

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## Introducción

Current evaluations of consciousness during anesthesia have limited precision. This can produce negative clinical consequences such as intraoperative awareness or neurological damage due to under- or over-dosage of anesthesia, respectively. Activity in frontal and parietal areas has been correlated to consciousness, including the modulation of consciousness through anesthetics.

## **Objetivo General**

This study aims to assess consciousness in wakefulness, deep sedation, and intermediate levels through biomarkers of electrical and hemodynamical brain activity.

## Material y Métodos

Volunteering patients undergoing an endoscopy or colonoscopy procedure are monitored during a stepped propofol infusion. We use a synchronized hybrid measurement system combining frontal and parietal electroencephalography (EEG) and parietal functional near-infrared spectroscopy (fNIRS). Five consciousness levels are defined using the Modified Ramsay Sedation Scale (MRSS) based on the patient's response to verbal, motor or painful stimuli.

The frequency spectrum bands and the oxygenated (HbO) and deoxygenated hemoglobin (HbR) fluxes are obtained from the EEG and fNIRS signals, respectively. In order to develop a machine learning algorithm capable of decoding levels of consciousness, the signals are divided into epochs of 8 seconds after the onset of each condition. From each epoch, the theta, alpha and beta frequency bands in EEG, and mean, peak and variance HbO and HbR in fNIRS, are used as features. These features are given to a supervised classifier, together with their assigned level of the MRSS.

## Resultados

As preliminary work, LDA classification models were trained with the parietal data of three subjects considering two conditions: resting state (baseline) and loss of consciousness (MRSS level 5). Two models were developed: EEG only and fNIRS only. Our preliminary models perform well, obtaining an F1 score of almost one when using EEG and significantly lower (near 0.7) for fNIRS. Both classifiers reached best performance using around 20 epochs from the trigger onset. As the number of epochs after the onset of the condition increases, the performance of the classifier decreases. The performance loss is abrupt after 80 and 50 epochs for EEG and fNIRS, respectively. Although the classifier was trained using few subjects and unbalanced data, the performance is above chance level. In the future, we seek to build a multi-class classifier using five consciousness levels and combined fNIRS-EEG data and an increased number of subjects.

## **Conclusiones y/o Implicaciones**

Anesthesiologists will benefit from the complementary information for better anesthesia induction. This can help prevent negative clinical consequences such as anesthesia overdosage and intraoperative awareness.

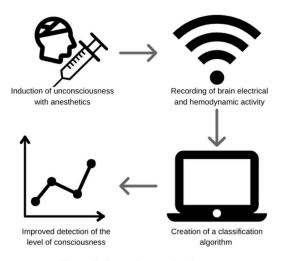
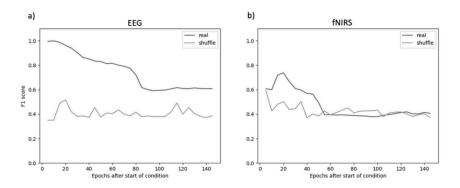


Figure 1. General research scheme





**Figure 2.** Classification performance (F1 score) for resting state and loss of consciousness using LDA for EEG (a) and fNIRS (b). For each epoch, features were fed to the LDA model. X-axes indicate the number of epochs. Y-axes represent the F1 score. Real and shuffle results are used to evaluate model overfitting.